

IDENTIFICATION OF MYOCARDIAL INFARCTION TISSUE BASED ON TEXTURE ANALYSIS FROM ECHOCARDIOGRAPHY IMAGES

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ABSTRACT

Texture is an important characteristic that can be used for identification and detection for surface defect or abnormalities. This research has an algorithm for identifying heart with suspected myocardial infarction problem based on texture analysis applied on echocardiography images. Texture tissue sample images taken from echocardiography sub-image (ROI). There are two tissue classes: Type 1 corresponds to normal myocardial tissue, whereas Type 2 corresponds to infarcted myocardium with small dimension. Therefore, in order to investigate possible differences tissue between patient with infarction tissue or not, we proposed a Wavelet Extension Transform and Gray Level Co-occurrence matrix.

Wavelet Extension Transform is used to form an image approximation with higher resolution. The gray level co-occurrence matrices are computed for each sub-band. The feature vector of testing image and other feature vector as normal image classified by Mahalanobis distance to decide whether the test image is infarction or not. The method is tested with real data from echocardiography images of human heart. For each patient to be analyzed tissue samples are taken from not-affected area and tissue samples are taken from image segments corresponding to the infarcted area of myocardium. The result of this experiment can detect difference image from echocardiography as normal myocardium and infarcted myocardial tissue.

Keywords: *Wavelet Extension, Infarction, Myocardial tissue, Co-Occurrence matrices*

1. INTRODUCTION

Textures provide important role for automatic visual inspection. The ability to represent is the single most important step in the development of system for measuring the similarity of textures and segmenting images on the basis of differences in textures. Their analysis is fundamental to many applications such as industrial monitoring of product quality control, remote sensing of earth resources, and medical diagnosis with computer tomography. Much research work has been done on texture analysis, such as classification, compression, retrieval and segmentation for last three decades. Despite the effort, texture analysis is still considered an interesting but difficult problem in image processing [4], [6],[11],[12].

Acute myocardial infarction is caused by the obstruction of a coronary artery by a thrombus, leading to irreversible damage of the heart muscle (myocardium). Echocardiography is a diagnostic test that uses ultrasound waves to create an image of the heart muscle. It may show such abnormalities as poorly functioning heart valves or damage to the heart tissue after acute myocardial infarction. Texture characteristic of ultrasound image is low quality, caused by noise, low frequency and small dimension.

Wavelet extension algorithm is proposed for improving quality of texture result of new image with higher resolution. Aleksandra Mojsilovic *et.al* [9] showed that, from the texture characterization perspective, the proposed decomposition scheme performs more efficient energy distribution of an image, and the first-order, second-order, and higher-order statistics calculated on the expanded images can be used as reliable texture description for classification purpose. Gray level co-occurrence matrix, one of the most known texture analysis methods, estimates image properties related to second order statistics. Mari Patrio *et.al.*[14] have used the feature extracted from GLCM with the problem of how to guarantee even quality within a set of rock plates. A.L. Amer *et.al.*[10] proposed a method, namely, the sub-band domain co-occurrence matrix to solved the texture defect detection problem. Therefore, this research proposed a new combines concept of wavelet extension transform with GLCM texture feature were used for diagnosis of myocardial infarction tissue and retrieval in small dimension images

The goal of this paper is to establish the algorithms for texture analysis, which can be detected by texture image as distinguishing a textural normal myocardium from textural infarcted.

This paper is organized as follow. Section II introduces background theory of wavelet and co-occurrence matrix. Experimental results are present in section III, and finally, in section IV, includes the concluding remarks.

2. METHODOLOGY

The proposed defect detection and texture retrieval system consist of two stages [10]: (i) The feature extraction part which first utilizes the wavelet extension procedure to decompose textured image into sub-bands and GLCM procedure to computed energy, entropy, contrast and inverse difference moment for each sub-bands (ii) The detection part (texture classification) which is a mahalanobis distance classifier being trained by defect free samples (see fig.1).

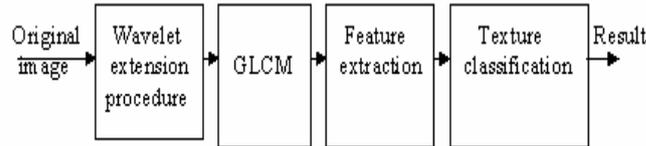


Figure 1: Block diagram

A. Review of Wavelet Transform

The wavelet transform is define as a decomposition of signal $f(t)$ with a family of real orthonormal bases $\psi_{m,n}(t)$ generated from a kernel function $\psi(t)$ by dilations and translations [5],[8],[13]:

$$\psi_{m,n}(t) = 2^{-m/2} \psi(2^{-m}t - n) \quad (1)$$

where j and k are integers.

The multiresolution formulation needs two closely related basic functions. In addition to the mother wavelet $\psi(t)$, we will need another basic function, called the scaling function $\phi(t)$. $\phi(t)$ can be expressed in term of weighted sum of shifted $\phi(2t)$ as [3]:

$$\phi(t) = \sqrt{2} \sum_k h(k) \phi(2t - k) \quad (2)$$

where $h(k)$'s are the scaling function (lowpass) coefficients and the mother wavelet $\psi(t)$ is related to the scaling function via

$$\psi(t) = \sqrt{2} \sum_n g(k) \phi(2t - k) \quad (3)$$

where $g(k)$'s are the wavelet (highpass) coefficients. They are required by orthogonality to be related to the scaling coefficients by

$$g(k) = (-1)^k h(1-k) \quad (4)$$

The mother wavelet $\psi(t)$ is good at representing the detail and high-frequency parts of a signal. The scaling function $\phi(t)$ is good at representing the smooth and low-frequency parts of the signal.

The 1-D multiresolution wavelet decomposition can be easily extended to two dimensions by introducing separable 2-D scaling and wavelet functions as the tensor product of their one-dimensional complements.

$$\begin{aligned} \phi_{LL}(x, y) &= \phi(x)\phi(y) \\ \psi_{LH}(x, y) &= \phi(x)\psi(y) \\ \psi_{HL}(x, y) &= \psi(x)\phi(y) \end{aligned}$$

$$\psi_{HH}(x, y) = \psi(x)\psi(y)$$

The corresponding filter coefficient are

$$f_{LL}(x, y) = h(x)h(y)$$

$$f_{LH}(x, y) = h(x)g(y)$$

$$f_{HL}(x, y) = g(x)h(y)$$

$$f_{HH}(x, y) = g(x)g(y)$$

where the first and second subscripts denote, respectively, the lowpass and highpass filtering along the row and column direction of the image.

Figure 2 shows how to implement the wavelet decomposition of an image. After the decomposition, four subbands, LL, LH, HL and HH subbands, which represent the average, horizontal, vertical, and diagonal information respectively.

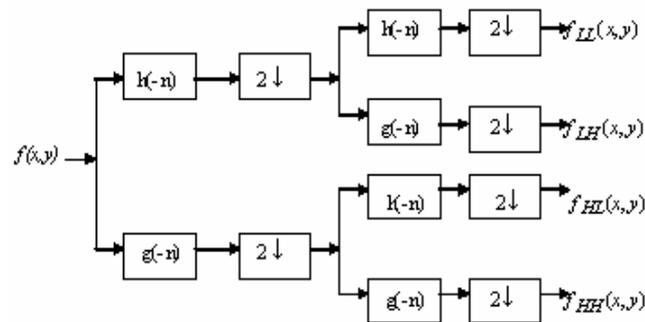


Figure 2: One stage in multiresolution image decomposition

In order, we use a procedure called wavelet image extension. The application of the procedure is illustrated by the block diagram in Figure 3a. These four images are used as the input into the extension (interpolation) procedure, which is illustrated by the block diagram in Figure 3b.

B. Co-occurrence Matrices

The co-occurrence matrix is defined by a distance and an angle, and its mathematical definition is

$$P_d[i, j] = |\{[r, c] : I[r, c] = i \text{ and } I[r + dr, c + dc] = j\}|$$

where d be a displacement vector (dr, dc) specifying the displacement between the pixel having values i and the pixel having value j , dr is a displacement in rows (downward) and dc is a displacement in columns (to the right) and I denote an image of size $N \times N$ with G gray values [10].

Texture classification can be based on criteria (feature) derive from the occurrence matrices.

1). Entropy

$$ENT = -\sum_i \sum_j p(i, j) \log p(i, j) \quad (5)$$

2). Contrast

$$CON = \sum_i \sum_j (i - j)^2 p(i, j) \quad (6)$$

3). Angular Second Moment

$$ASM = \sum_i \sum_j \{p(i, j)\}^2 \quad (7)$$

4). Inverse Difference Moment

$$IDM = \sum_i \sum_j \frac{1}{1+(i-j)^2} p(i, j) \quad (8)$$

In Equation (5) – (8), $p(i, j)$ refers to the normalized entry of the co-occurrence matrices. That is

$$p(i, j) = \frac{p_d(i, j)}{R} \quad (9)$$

where R is the total number of pixel pairs (i, j) . For a displacement vector $d = (dr, dc)$ and image of size $N \times M$ R is given by $(N-dr)(M-dc)$.

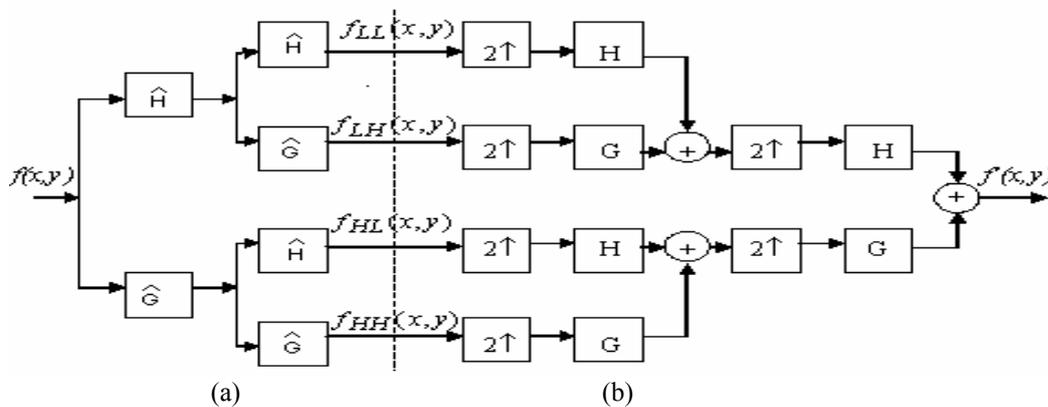


Figure 3: Block diagrams illustrating the complete wavelet decomposition-extension procedure (a) the composition part and (b) the extension (synthesis) algorithm.

3. EXPERIMENTAL RESULTS

The experiments in this part are used texture image from ultrasound images taken from 15 patients, obtained from clinical hospital. For each patient to be analyzed, five tissue samples are taken from ultrasound image segments corresponding to area not affected (2) by infarction, and five tissue samples taken from image segments corresponding to the infarcted (1) area of myocardium.

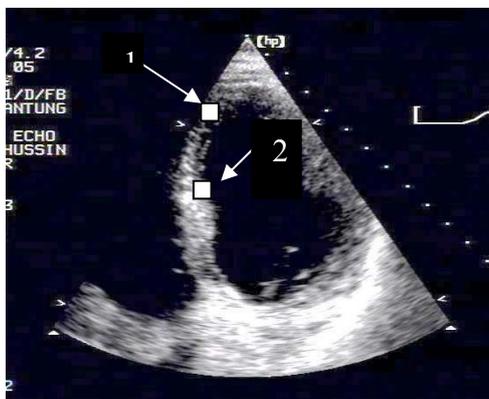


Figure 4: A typical ultrasound image of a human heart. The black square correspond to texture sample taken from a normal area (1) and an indicated infarcted area of myocardium (2).

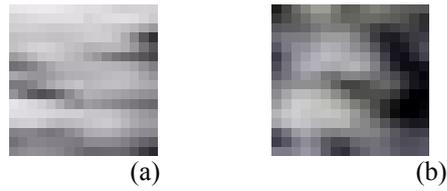


Figure 5: a. Normal myocardium zone (16x16), b. Infarcted myocardium zone (16x16).

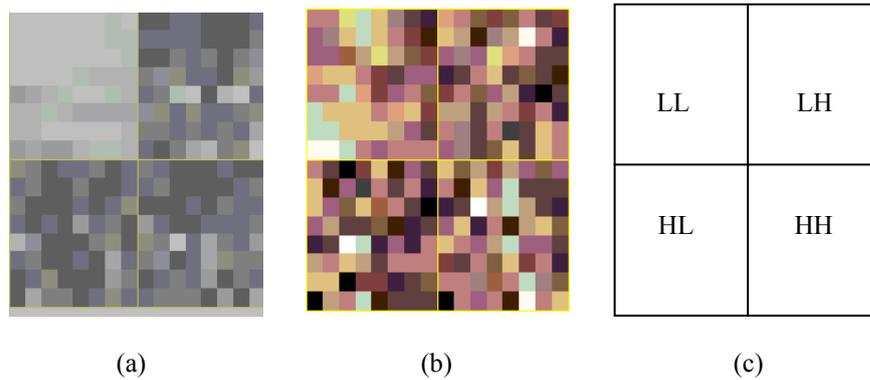


Figure 6: a. Wavelet decomposition of normal myocardium, b. infarcted myocardium, and c. the arrangement of the four subbands (LL is low-frequency content of the original picture, LH gives the horizontal high frequencies, HL corresponds to vertical high frequencies and HH the high frequencies in both directions).

TABLE 1: Distance value (D) between normal and infarcted zones, Threshold value $\alpha = 2.7461$.

| Patient | D |
|-----------------|---------|
| Infarcted Group | |
| P1 | 3.15040 |
| P2 | 3.02680 |
| P3 | 3.74600 |
| P4 | 4.49660 |
| P5 | 2.81280 |
| P6 | 2.87220 |
| P7 | 2.75430 |
| P8 | 3.88320 |
| P9 | 3.09640 |
| P10 | 4.18970 |
| Normal Group | |
| P11 | 0.49733 |
| P12 | 0.98083 |
| P13 | 1.06870 |
| P14 | 1.71170 |
| P15 | 0.39482 |

4. CONCLUSIONS

The following conclusions can be drawn from our studies:

- 1). Algorithm for texture analysis has advantage for detect difference image from echocardiography as normal myocardium and myocardium infarction.
- 2). Wavelet extension and co-occurrence matrix procedure approach is an effective method for application in similarity evaluation of texture images.

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